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(11) (A) NO. 1 158 988

(45) ISSUED 831220

(52) CLASS 182-13

(51) INT. CL. ³ A61K 35/16 B01D 13/00

(19) (CA) **CANADIAN PATENT** (12)

(54) METHOD AND APPARATUS FOR LOW PRESSURE FILTRATION
OF PLASMA FROM BLOOD

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(21) APPLICATION NO. 363,280

(22) FILED 801027

(30) PRIORITY DATE U.S.A. (118,677) 800205

NO. OF CLAIMS 12

Canada

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CCA-274 (11-62)

ABSTRACT OF THE DISCLOSURE

A method and apparatus for carrying out separation of plasma from whole blood, in which whole blood is passed through a filtration membrane means of a material suitable for separating plasma from whole blood and having a pore size from 0.1 to 0.6 microns at positive pressure differential across the membrane in a range up to just below 50 mm Hg. This provides an increased flow as compared to the flow obtained with higher pressure differentials.

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This invention relates to a method and apparatus for separating blood plasma from whole blood, i.e. blood from a person or animal, and more particularly to such a method and apparatus which operates at a relatively low pressure and yet obtains an improved quantity of separated plasma.

Until relatively recently, the separation of plasma from whole blood, such as for the purpose of utilizing the plasma from a donor for transfusion to others or for some sort of treatment of the blood, has been carried out by extracting the whole blood and centrifuging it to separate the plasma. Such procedures are not only time-consuming and cumbersome requiring large amounts of manual and mechanical handling, but they require a relatively large amount of expensive equipment.

Recently investigations have been conducted into so-called on-line membrane plasma separation techniques. In this type of separation, the blood is passed through the on-line separation equipment and immediately returned to the donor, the plasma being separated, and in the case of a donor, collected and stored, or alternatively in a case of a patient, treated such as by sorption of a solute which it is desired to remove, and then returned to the patient. In addition to being much simpler than the centrifugal techniques of plasma separation in terms of the manual and mechanical handling of the blood, and lower expense, this technique when used for the treatment of the plasma has advantages over the conventional treatment of solute removal which incorporate treating agents in direct contact with whole blood in that in many instances the solute which it is desired to remove is



concentrated in the plasma, making the technique a rapid and simple way to cleanse the blood. The most suitable treatment material can be chosen and used for the particular treatment desired without the need to consider the effect of the treatment material on the blood cells, since blood cell-treating agent interaction are eliminated, multiple types of treating agents may be employed and it is easy to filter the treatment material from the plasma before reinfusing it into the patient, thus providing a treatment methodology that is safe in a wide variety of applications.

One method of carrying out such a plasma separation technique and an apparatus therefor are disclosed in United States Patent No. 3,705,100 to Blatt, et al. A membrane arrangement is shown in which the pore sizes are 0.1 to 0.8 microns, and the blood is passed over the surface of the membrane at a flow rate of 2-50 feet per minute while a pressure differential across the membrane is maintained at from 1 to 15 psi. This method and apparatus are said to be effective in separating the plasma from the whole blood.

A similar method is disclosed in K. Ouchi et al, An Efficient, Specific and Blood Compatible Sorbent System for Septic Assist, Vol. XXIV Transactions American Society Artificial Internal Organs 246, 1978, in which a cellulose acetate filter was used to separate plasma from whole blood flowing through hollow fiber membranes at a rate of 100 ml/min. and at pressure differentials across the membrane of 60, 100 and 137 mm Hg., the plasma separation rate at each of these pressures being 37 ± 2 ml/min, 34 ± 2 ml/min

and 32 \pm 2 ml/min respectively.

Recently issued United States Patent No. 4,191,182 to Popovich et al also discloses a method and apparatus for continuous separation of plasma by so-called ultra-filtering. As with the above-described prior art, Popovich et al also operate at transmembrane pressures in the 50-700 mm Hg. range. While recognizing that transmembrane pressures which are too high will cause damage to the cellular components of the blood and that control of transmembrane pressure is necessary to avoid clogging of the filter, Popovich et al nevertheless prefer to operate in the 100-400 mm Hg. range of transmembrane pressures.

The present invention provides a method of separating blood plasma from whole blood, i.e. blood from a healthy and/or diseased person or animal, which method has advantages over the prior art method, yet which operates at a lower transmembrane pressure than the prior art methods so as to avoid problems of damage to cellular components of the plasma and clogging of the filter.

The invention also provides an apparatus for carrying out this method.

According to the present invention, it has been found that, contrary to normal expectations, by operating at a positive transmembrane pressure differential up to just below 50 mm Hg., and particularly from about 8.5 mm Hg. up to just below 50 mm Hg., the filtration rate of the plasma can be increased as compared with filtration rates when operating above 50 mm Hg. The advantages of the invention are thus achieved by directing a flow

of whole blood across one face of a filtration membrane means comprising a material suitable for separating plasma from whole blood and having a pore size from 0.1 to 0.6 microns, said flow being at a flow velocity of from 5 to 1500 cm/min and being at a depth sufficient for separating plasma from the flow of blood, while at the same time generating a positive pressure differential across said membrane up to just below 50 mm Hg. for forcing plasma through the membrane, and collecting the plasma separated by the membrane. Preferably the pressure is in a range of from about 8.5 mm Hg up to just below 50 mm Hg. More preferably, the pressure is in a range of from about 20 mm Hg. to about 40 mm Hg.

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This is different from conventional ultrafiltration, in which it is generally considered that the filtration rate increases with an increase in transmembrane pressure. The present invention demonstrates that the usual considerations do not apply in filtration of plasma from whole blood, possibly due to the complex mixture of particles in blood.

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It has also been discovered that there is a further advantage in the plasma separation when it is carried out at such low transmembrane pressures. Plasma is an extremely complex fluid containing many solutes the molecules of which have different sizes. Current developments in the plasma filtering art are judged not only by the quantity of plasma which can be filtered, but by the quality or composition of the filtrate, one measure of which is the sieving coefficient, namely the relative amounts of desired components of the plasma present in the filtrate as compared to the amounts of such components present in the blood from which the

plasma is filtered. The present inventors have found that not only is the quantity of plasma which can be filtered from whole blood increased by operating at the low positive transmembrane pressures, but also the sieving coefficient for the various components of the plasma is increased.

The apparatus according to the invention for carrying out separation of plasma from whole blood comprises a filtration membrane means of a material suitable for separating plasma from whole blood and having a pore size from 0.1 to 0.6 microns; means 10 for directing a flow of whole blood across one face of said membrane at a flow velocity of from 5 to 1500 cm/min and at a depth sufficient for enabling separation of plasma from the flow of blood; means for generating a positive pressure differential across said membrane up to just below 50 mm Hg., for forcing the plasma through the membrane; and means for collecting the plasma separated by the membrane. Preferably the positive pressure differential across said membrane ranges from about 8.5 mm Hg. up to just below 50 mm Hg. The membrane means can be a film type membrane or a hollow fiber membrane, for example of cellulose acetate.

20 Other and further features of the invention will become apparent from the following detailed description, taken with the accompanying drawing, in which:

Figure 1 is a schematic diagram of an apparatus for separating blood plasma from whole blood, collecting it and then either treating it, and returning it to the patient after proper filtering, or forwarding it to storage or further use; and

Figure 2 is a graph of transmembrane pressure vs. plasma filtration rate according to the method of the present invention.

Figure 1 shows schematically an apparatus for carrying out the method of the invention. The apparatus comprises an inlet blood pump 10 to the inlet of which a line or tube 11 from a patient or donor is connected and which has a tube 12 extending from the outlet thereof through a bubble trap 12a to the inlet to a plasma filter 13. From the downstream end of the plasma filter 13 a further line 14 extends to a bubble trap 15 and a line 16 extends from the bubble trap back to the patient. From the filtrate side of the filter 13 a line 17 extends to a plasma reservoir 18 and a line extending from the outlet of the plasma reservoir is connected to a plasma pump 19 the outlet of which is in turn connected to a three-way valve 20. Extending from one outlet to the valve 20 is a line 23 leading to collection means or the like for collecting the plasma for further use, or to some other part of the apparatus for treating the plasma for further use. The other outlet of the three-way valve is connected to a treatment means, such as a sorbent cartridge 21, the outlet of which is in turn connected to a particle filter 22 and through the particle filter to the bubble trap 15.

This arrangement can be modified. For example, the plasma reservoir 18 can be incorporated into the plasma filter 13. The reservoir need not be vented, in which case the pumping speed of the plasma pump 19 can be regulated to regulate the plasma reservoir pressure and therefore also the transmembrane pressure across the filter element or filter means of the plasma filter 13.

The various parts of the apparatus are mostly conventional, such as the blood pump, the plasma reservoir, the plasma pump, the sorbent cartridge, the particle filter and the bubble traps. The plasma filter can be any one of a plurality of known types of filters. The filter has membranes of a material which is not affected by whole blood or any of the materials contained therein and which is thus suitable for filtration of plasma from blood. A number of materials are available for use as such membranes, such as hydrophilic materials such as cellulose acetate, cuprophane* or cellophane as disclosed in United States Patent No. 4,031,010 to Nose, or polycarbonate or polypropylene, but the preferred materials are polycarbonate such as Nuclepore* 040 sold by Nuclepore Corp., and cellulose acetate. The pore size should be from 0.1 to 0.6 microns. The arrangement of the membranes in the filter can be any arrangement suitable for producing a pressure differential across the membrane which causes the plasma to be filtered out as the whole blood flows across the surface of the membrane. A number of other such arrangements can be found in the art. These can be generally divided into parallel film type membrane arrangements, such as shown in the Nose Patent, and hollow fiber arrangements. In the parallel plate arrangements, the space on one side of the parallel plate membranes is connected to the blood inlet and outlet of the filter and the space on the other side of the membrane is connected to the filtrate outlet of the filter. In the hollow fiber arrangements, the fibers are mounted in the filter so that the space within the fiber is

*Trade mark

connected between the blood inlet and outlet of the filter and the space around the fiber is connected to the filtrate outlet, or vice versa although the preferred embodiment is with blood flow through the interior of the fiber. The hollow fibers which are particularly suitable are cellulose acetate hollow fibers sold by Asahi Medical Co., Tokyo, Japan. The advantages of this type of membrane over the plate type are that the hollow fiber geometry is inherently strong enough so that no dimensional change occurs at transmembrane pressure necessary to obtain required plasma flows, that due to this structural strength, no additional support structure is necessary, and that because no support structure is necessary, the overall filter structure is simpler and less costly. This is particularly important in light of the strong influence fluid dynamic conditions play upon filtration rate and sieving properties.

Where the apparatus is to be used simply to collect plasma, the three-way valve 20 is turned so that the plasma from the plasma reservoir is discharged to some conventional plasma collection means. Where the apparatus is to be used to treat the separated plasma and return it immediately to the patient, the three-way valve 20 is turned so that the plasma from the reservoir is directed through the treatment, e.g., absorption cartridge 21 to the particle filter 22 and bubble trap 15, whereafter having been filtered to remove any of the treatment particles, the plasma is recombined with the whole blood from line 14.

Where the apparatus is to be used for treating the separated plasma, the sorbent in the cartridge 21 can be any sorbent which is effective for removing the unwanted material from the plasma. United States Patent No. 4,013,564 to Nose suggests several types of sorbents.

It has been found that with the apparatus as described above, by operating it under certain conditions of blood flow and transmembrane pressure, a plasma filtration rate for separating plasma from normal blood which is unexpectedly high
10 can be obtained and also sieving coefficients can be increased. The blood flow rate through the filter should be such that the flow velocity of the blood across the one face of the membrane is from 5 to 1500 cm/min. The inlet blood pump 10 and the size of the filter should be such that, under the downstream pressure conditions due to directing the blood back to the patient, and the pressure conditions on the plasma side of the filter element or filter means is such, i.e. either atmospheric as in a so-called open system, or a pressure controlled such as by the pump 19, as to be below the pressure on the blood side
20 of the filter, the transmembrane pressure is a positive pressure up to just below 50 mm Hg., and particularly from about 8.5 mm Hg. to just below 50 mm Hg. Preferably the system is operated so that the pressure range is from 40 to 20 mm Hg. When this is done, the plasma filtration rate, i.e., the rate at which plasma is filtered out of the blood through the membrane, is a maximum. By positive transmembrane pressure is meant a transmembrane pressure which is the difference between a higher pressure on the whole

blood side of the filter and a lower pressure on the plasma side of the filter.

In order to demonstrate the improved plasma filtration rate, a series of experiments were carried out on dogs, the blood of which was sufficiently similar to whole blood with a substantially normal protein content to provide a useful indication of how the method and apparatus will operate with humans. In each experiment the blood was extracted from the dogs and passed through the system as shown in Figure 1 under conditions within the ranges set forth above. The pressure on the plasma side of the filter element was atmospheric so that the apparatus is considered to be a so-called open system.

10 Three normal dogs were perfused a total of seven times, three times using an N type plasma filter, and four times using an S type filter 13 of Figure 1.

The two types of filters were both hollow fiber cellulose acetate type filters and corresponded to those available from Asahi Medical Co., Tokyo, Japan, under the trademark PLASMAFLO the fibers having an inside diameter of 370 μm , a wall thickness of 190 μm , a porosity of 84% and a nominal pore size of 0.2 μm the N type filter having 2500 fibers with an effective fiber length (potting to potting in the fiber structure) of 240 mm, and a surface area of about $.7\text{m}^2$, and the S type filter having 3300 fibers with an effective fiber length of 200 mm and a surface area of about $.75\text{m}^2$. The blood tubing used to supply the blood from the dogs to the filter apparatus and to connect the parts of the filter apparatus with each other was tubing sold

under the trade mark Lifemed by Lifemed Division of Vernitron, Compton, California. The priming volume of the apparatus was about 400 ml. Blood access was via the femoral or internal carotid artery and blood was reinfused via the femoral or jugular vein through FC-100 cannulae sold by Extracorporeal Medical Co., Inc. King of Prussia, Pennsylvania. Systemic heparinization was used in each perfusion, 2 mg/kg heparin (A. H. Robins, Richmond, Virginia) being injected prior to starting perfusion and 0.5 mg/kg/hr for the rest of the perfusion.

10 An inlet blood flow of 100 ml/min was maintained by the pump 10, which was a low amplitude pulsatile flow roller-pump sold by Drake-Willcock Co., Ltd. which was sufficient to cause a velocity of flow across the membrane of about 25-40 cm/min. The rate of plasma filtration, the inlet and outlet pressures of the filter and the sorbent cartridge were determined for each perfusion. The transmembrane pressures and flow rates were as shown plotted in Figure 2.

20 Contrary to the situation normally encountered when filtering a liquid material through a filter in which the flow of filtered liquid across the filter falls with a drop in transmembrane pressure, it will be seen from Figure 2 that the amount of plasma which is filtered through the membrane actually increases below pressures heretofore considered a minimum satisfactory transmembrane pressure for filtering plasma, reach a peak at about 30 mm Hg. of transmembrane pressure before falling off. From this Figure it can be seen that the most advantageous transmembrane pressures for achieving the maximum filtration of

plasma from normal whole blood lie in the range of from just below 50 mm Hg. to about 8.5 mm Hg. with the best pressures in the range of from about 40 to about 20 mm Hg.

While the data point at the lowest transmembrane pressure shows a plasma flow rate near the maximum, the transmembrane pressure of 8.5 mm Hg. for this point is not a precise pressure for this flow rate. The pressures below 10 mm Hg. cannot be known with any great accuracy because of the utilization of the low amplitude pulsatile flow roller pump and the nature and accuracy of interpretation of the instruments used for the various measurements. The pump does not, as its name makes clear, operate at a steady pressure. It had an amplitude of pressure from the lowest pressure to the highest on the order of 10 mm Hg., which is conventional for plasma separation from blood, and the transmembrane pressures for the respective data points were calculated using the mean value of the pump pressure. Thus the lower pump pressure and thus the transmembrane pressure is somewhat lower than the mean value, possibly as low as about 3.5 mm Hg. Moreover, the pressure gauges used had an accuracy of ± 2 mm Hg. at best. Further, the fluid level at the pressure monitoring points was fluctuating, and the column heights of mercury were varying during the pressure readings. For the higher transmembrane pressures, these factors are not very significant, but for those from 10 mm Hg. down, this is very significant. All of these factors together indicate that the transmembrane pressure can be a positive

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transmembrane pressure near zero and still produce a very high plasma flow as compared to what might normally be expected. The pressures at which the present method is operable is therefore a positive transmembrane pressure up to just below 50 mm Hg. Moreover, due to these factors, the numerical value of 8.5 mm Hg. for the transmembrane pressure for the plasma flow data point at the lowest transmembrane pressure is only approximate, and in fact may be considerably lower. For this reason, the numerical limit on the transmembrane pressure as set forth in the specification and claims is expressed as "about" 8.5 mm Hg., and this expression is intended to include somewhat lower pressures due to the factors discussed hereinabove.

THE EMBODIMENTS OF THE INVENTION IN WHICH AN EXCLUSIVE PROPERTY OR PRIVILEGE IS CLAIMED ARE DEFINED AS FOLLOWS:

1. An apparatus for carrying out separation of plasma from whole blood, comprising:
 - a filtration membrane means of a material suitable for separating plasma from whole blood and having a pore size from 0.1 to 0.6 microns;
 - means for directing a flow of whole blood across one face of said membrane at a flow velocity of from 5 to 1500 cm/min and at a depth sufficient for enabling separation of plasma from the flow of blood;
 - means for generating a positive pressure differential across said membrane up to just below 50 mm Hg. for forcing the plasma through the membrane; and
 - means for collecting the plasma separated by the membrane.
2. An apparatus as claimed in claim 1 in which said means for generating a positive pressure differential across said membrane generates a pressure in a range from about 8.5 mm Hg. to just below 50 mm Hg.
3. An apparatus as claimed in claim 1 in which said membrane means is a film type membrane.
4. An apparatus as claimed in claim 1 in which said membrane means is a hollow fiber membrane.
5. An apparatus as claimed in claim 1 in which said membrane means is a hollow fiber membrane of hydrophilic material.

6. An apparatus as claimed in claim 1 in which said pressure generating means comprises means for generating a pressure differential across said membrane in a range of from about 20 mm Hg. to about 40 mm Hg.

7. A method of separating plasma from whole blood, comprising the steps of:

directing a flow of whole blood across one face of a filtration membrane means comprising a material suitable for separating plasma from whole blood and having a pore size from 0.1 to 0.6 microns, said flow being at a flow velocity of from 5 to 1500 cm/min and being at a depth sufficient for separating plasma from the flow of blood,

and at the same time generating a positive pressure differential across said membrane up to just below 50 mm Hg. for forcing plasma through the membrane, and

collecting the plasma separated by the membrane.

8. A method as claimed in claim 7 in which the step of generating a pressure differential across said membrane comprises generating a pressure in a range from about 8.5 mm Hg. to just below 50 mm Hg.

9. A method as claimed in claim 7 in which the pressure generating step comprises generating a pressure in a range of from about 20 to about 40 mm Hg.

10. A method as claimed in claim 7 in which said membrane means is a film type membrane.

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11. A method as claimed in claim 7 in which said membrane means is a hollow fiber membrane.

12. A method as claimed in claim 7 in which said membrane means is a hollow fiber membrane of hydrophilic material.

FETHERSTONHAUGH & CO.

PATENT AGENTS

OTTAWA, CANADA

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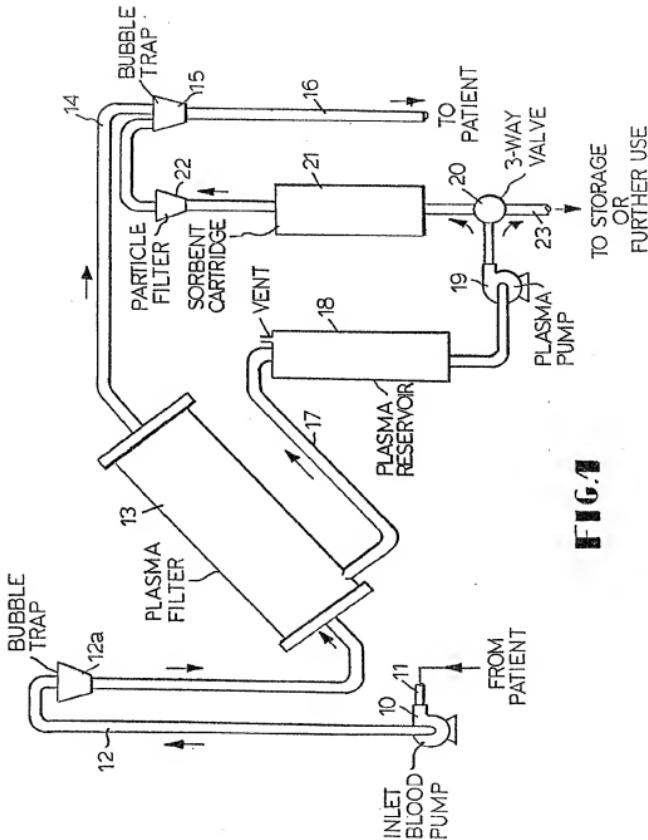


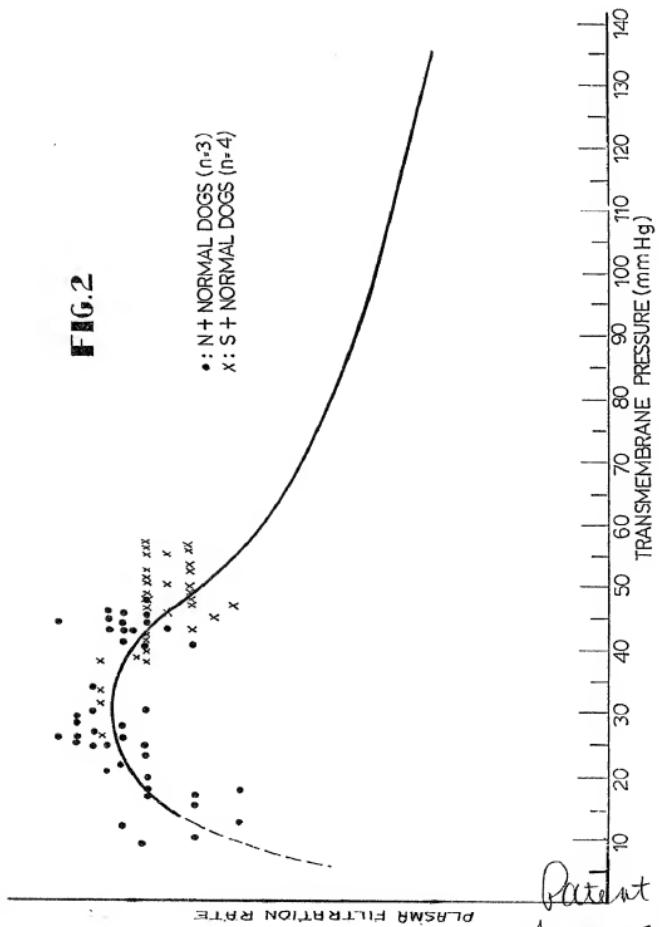
FIG. 1

Patent Agents
Jetherstonhaugh & Co.

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FIG. 2



Patient Agents
Jetterstonhaugh, L.